Ion implantation dose high-resolution monitoring in Si wafers using laser infrared photothermal radiometry with lock-in common-mode-rejection demodulation

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Abstract

Frequency-scanned and lock-in common-mode-rejection demodulation schemes were used with laser infrared photothermal radiometric (PTR) detection of B +, P +, and As + ion-implanted Si wafers, with or without surface-grown oxides. The implantation energy was 100 keV with doses in the range $1 \times 10^{11}$–$1 \times 10^{13}$ ions/cm$^2$. The lock-in common-mode-rejection demodulation (CMRD) scheme exhibited superior signal resolution in all cases where the conventional frequency-scan signals were essentially overlapped. These were B+-implants in the dose range $1 \times 10^{12}$–$1 \times 10^{13}$ ions/cm$^2$, and P+-implants in the $10^{12}$ ions/cm$^2$ range.

Very recently a novel harmonic common-mode-rejection (CMR) lock-in amplifier (LIA) pulse waveform demodulation scheme was introduced [1,2]. This particular repetitive waveform is shown in Fig. 1. It takes advantage of the details of the demodulation mechanism in conventional lock-in amplifiers [3], resulting in complete suppression of baseline signals. The demodulated LIA signal output expected from an input double square waveform of equal durations $\tau_1 = \tau_2$, is ideally zero. This occurs because the demodulated LIA output signal with a long filter time-constant compared to the waveform repetition period, is the time-integral (area) of the input waveform during the first half cycle minus the integral (area) of the input waveform during the second half cycle [3]. For identical half-waveforms and zero instrumental phase delay (alignment of the LIA reference square-wave rising edge with the onset of the external incident waveform), this signal generation scheme implies that equal areas are swept along the time axis. Therefore, the result of the signal demodulation (integral/area subtraction between $[0,T/2]$ and $[T/2,T]$ segments) is zero for all types of waveforms. This signal generation principle can be thought of as the temporal analog of destructive interference due to spatial superposition of two out-of-phase waves. The main advantage of CMR demodulation (CMRD) is the suppression of LIA signal baselines, which, in turn, enhances the dynamic range of the instrument. An application of CMRD to photothermal radiometric detection [2] has shown considerable measurement resolution improvement in cases where minute changes in sample thermophysical properties produce only very small signal differences. These differences are usually imperceptible under conventional square- or
Fig. 1. CMRD optical excitation waveform consisting of a bi-modal pulse applied to the acousto-optic modulator of a laser photothermal radiometric system. The horizontal time units are expressed as percentage of a full repetition period $T$; $\tau_1$ and $\tau_2$ are the corresponding square pulsewidths, and $\Delta$ is the center-to-center pulse separation. Only one repetition period is presented for clarity.

A typical set of amplitude response curves from near the center of the five unoxidized P$^+$-implanted wafers examined in this work is shown in Fig. 2. PTR phase curves have not been used because they are more poorly resolved with respect to implantation dose than the associated amplitudes. The low-frequency slopes in Fig. 2 are due to thermal-wave domination of the signal as a result of lattice damage by the implantation process. In the 1–100 kHz range, the photo-excited carrier plasma-wave dominates the PTR signal. The amplitude depends on the depth integral of the free-carrier-density wave, and, in principle, it decreases monotonically with increasing implantation dose, as a result of enhanced recombination and trapping of photo-excited carriers at electronic defect states and traps, the density of which also increases with ion implantation dose [7]. Variations in ion-implanter parameters, however, generate non-uniform implant distributions across a wafer and diffusion-wave techniques such as PTR and MTR are sensitive to these variations [8]. In Fig. 2 it is clearly seen that signal resolution is severely compromised for doses above $4 \times 10^{11}$ cm$^{-2}$, with the curves corresponding to $1 \times 10^{12}$ cm$^{-2}$ and $4 \times 10^{12}$ cm$^{-2}$ being essentially unresolved. Furthermore, for that particular coordinate point near the wafer center, the signal amplitude for the wafer implanted with $1 \times 10^{13}$ cm$^{-2}$ is higher than those with the two next lower doses. This trend was consistent with signals obtained from other coordinate points on these wafers. The size of experimental error bars was that of the data points in Fig. 2 and subsequent figures. Monotonic amplitude decreases with increasing dose were found, as expected, for the remaining wafers, with the exception of the B$^+$ wafer implanted with $4 \times 10^{12}$ cm$^{-2}$, which showed significant amplitude increase over both the $1 \times 10^{11}$ cm$^{-2}$ and the $1 \times 10^{13}$ cm$^{-2}$ wafers. The signals from these latter wafers (center points) were very close to each other, but
not totally overlapped. Fig. 3 is a summary of the experimental results from the entire set of wafers at 4 kHz, a frequency at which implant dose resolution was found to be optimal for all PTR frequency scans such as those of Fig. 2. No PTR amplitude transients were observed under the laser probe, with the exception of the anomalous 1 \times 10^{11} \text{ cm}^{-2} \text{ P}^+ - \text{ and B}^+ - \text{implanted wafers}. These samples exhibited very mild positive transients, slowly (~2000 s) saturating to the steady-state signal values reported in Fig. 3. With the exception of the anomalous 4 \times 10^{12} \text{ cm}^{-2} \text{ B}^+ \text{ and } 1 \times 10^{13} \text{ cm}^{-2} \text{ P}^+ \text{ ion implants, the decreasing order of PTR amplitudes (B}^+, \text{P}^+, \text{As}^+) \text{ for the unoxidized wafers is consistent with the increasing degree of damage incurred to the Si lattice by the progressively larger ions. It is interesting to note the relative large restoration of PTR amplitude exhibited by the oxidized, As}^+ - \text{implanted wafers, as expected from the decreased defect density at the SiO}_2 - \text{Si interface [9].}

The CMRD technique was applied to each wafer at the same coordinate points as the frequency scans. The repetition frequency of 4 kHz was chosen for direct comparisons with the curves of Fig. 3. Waveform center-to-center scans (separation \delta t, Fig. 1) were performed with \tau_1 = 5 \text{ ms and } \tau_2 = 25 \text{ ms}. These pulse durations were chosen because they yielded maximum signal sensitivity. Each CMRD scan was preceded by a time-scan of the same coordinate point. It was found that the CMRD amplitude and quadrature signals were optimal in terms of dose resolution, compared to the CMRD phase and in-phase signals. Furthermore, it was established that for well-separated curves, such as those associated with the oxidized As}^+ - \text{implanted wafers, there was no discernible advantage to using the CMRD over the frequency-scanned method. This is reasonable, because for large dose-generated PTR signal changes the baseline suppression ability of the CMRD is limited by the natural signal differences among PTR curves. Fig. 4 shows time scans of the 4-kHz conventional PTR signal amplitudes from the P}^+ - \text{implanted wafers. Owing to the weak (or absent) transients, these traces are consistent with the order of amplitudes shown in Fig. 2 at the same frequency. The size of the increments \delta t \text{ controls the resolution of the technique as it limits its ability to suppress the signal baseline, i.e. to minimize the area between the } [0,T/2] \text{ and } [T/2,T] \text{ pulses. \delta t = 1% increments between 20% and 80% were used with only marginal improvement in resolving the overlapped P}^+ \text{ 1 \times 10^{12} \text{ cm}^{-2} \text{ and } 4 \times 10^{12} \text{ cm}^{-2} \text{ dose curves. Those scans were followed by \delta t = 0.3% — increment scans between 40% and 70%. The resulting curves are shown in Fig. 5. In comparison with Fig. 4, CMRD is shown to be capable of superior resolution of the 1 \times 10^{12} \text{ cm}^{-2} \text{ and } 4 \times 10^{12} \text{ cm}^{-2} \text{ dose curves. The } 4 \times 10^{11} \text{ cm}^{-2} \text{ curve is also included for comparison. The curves of Fig. 5 are the smoothed averages of three experimental runs each. Smoothing was performed either by taking the average over three consecutive points (discrete points) or by means of a sixth-order polynomial fit to the data (continuous lines). Smoothing may become necessary at high implant dose resolution signal levels, because the large baseline suppression of CMRD requires setting the LIA scale in the } \mu \text{V (instead of mV) range, where instrumental noise could be significant. The dose dependent CMRD-PTR amplitudes for P}^+ - \text{implantation decrease monotonically and are shown in Fig. 6. This curve is to be compared to the corresponding conventional frequency-scanned PTR dose dependence shown in Fig. 2.}

CMRD was further applied to the set of five B}^+ - \text{implanted wafers. The conventional PTR time scans at 4 kHz are shown in Fig. 7. In this case the } 4 \times 10^{12} \text{ cm}^{-2} \text{ and } 1 \times 10^{13} \text{ cm}^{-2} \text{ traces are poorly resolved,}
however, the dose resolution is somewhat higher than that of the foregoing P+ implants, Fig. 4. Accordingly, the CMRD technique (both amplitude and quadrature) was able to significantly improve the dose resolution of these two B+-implanted Si wafers by use of the relatively large pulse separation increment \( \delta A = 1\% \). There was no need to use finer \( \delta A \) increments for this case, with the concomitant advantage in signal-to-noise ratio over Fig. 5. The CMRD amplitudes are shown in Fig. 8, where it is observed that the amplitude order of the various curves is the same as that of the time traces of Fig. 7 and with the B+ curve of Fig. 3, including the “anomalously” high signal from the nominally implanted with \( 4 \times 10^{12} \) cm\(^{-2} \) wafer.

In summary, the CMRD-PTR method has been used with B+, P+, and As+, 100-keV ion-implanted Si wafers (the As+-implants with or without surface-grown oxides) in the implantation dose range \( 1 \times 10^{11} \)–\( 1 \times 10^{13} \) ions/cm\(^2\). This range is difficult to monitor with conventional laser-based photothermal probes, as some signals exhibit low sensitivity to dose. It was found that CMRD can significantly enhance the dose resolution of PTR response curves from B+ and P+ ion-implanted wafers in cases where conventional frequency scans were totally or partially unable to resolve the dose. In all other cases where frequency scans can resolve implantation doses, CMRD did not present any significant resolution advantages. It was further established that the pulse separation increment

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Fig. 5. PTR-CMRD amplitudes from the P+-implanted wafers of Figs. 2 and 4 vs. pulse separation \( A \) (%). Doses (ions/cm\(^2\)): (\( \triangleright \)) \( 4 \times 10^{11} \); (\( \triangle \)) \( 4 \times 10^{12} \); (\( \bigcirc \)) \( 4 \times 10^{13} \). Pulse separation increment \( \delta A = 0.3\% \).

Fig. 6. High-resolution CMRD amplitudes of P+-implanted wafers vs. implantation dose. \( \delta A = 0.3\% \).

Fig. 7. Conventional square-wave modulated PTR amplitude traces from the B+-implanted Si wafers at 4 kHz, as a function of time upon initial exposure to the laser beam. Doses (ions/cm\(^2\)): (\( \Box \)) \( 1 \times 10^{11} \); (\( \bigcirc \)) \( 1 \times 10^{11} \); (\( \bigtriangledown \)) \( 1 \times 10^{12} \); (\( \bigtriangledown \)) \( 4 \times 10^{12} \); (\( \bigtriangledown \)) \( 1 \times 10^{13} \).

Fig. 8. PTR-CMRD amplitudes from the B+-implanted wafers of Figs. 3 and 7 vs. pulse separation \( A \) (%), with \( \delta A = 1\% \). Doses (ions/cm\(^2\)): (\( \nabla \)) \( 1 \times 10^{11} \); (\( \bigcirc \)) \( 4 \times 10^{11} \); (\( \bigtriangleup \)) \( 1 \times 10^{12} \); (\( \nabla \)) \( 4 \times 10^{12} \); (\( \bigtriangledown \)) \( 1 \times 10^{13} \).
δd is the critical CMRD waveform parameter, which controls the dose resolution capabilities of the technique.

References